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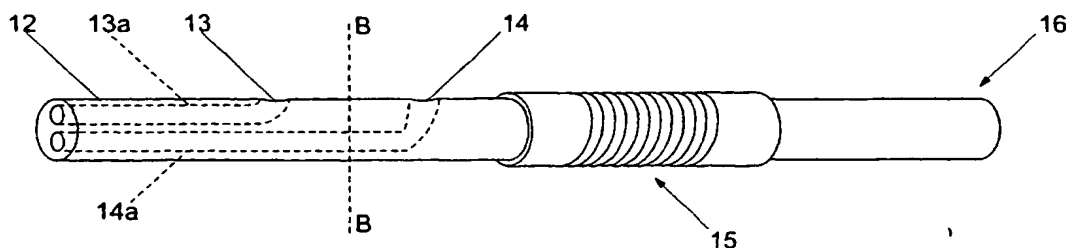
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(57) Abstract: A catheter which includes means to measure local pressure at two or more points along the catheter body is described. The points are preferably located in two different pressure areas, more preferably across a valve in a vessel, organ or similar. The invention provides a method of gauging the positional location of a catheter in a blood vessel, organ or similar, either by the catheter having means to monitor the local pressure at two or more points along the catheter body, or means to measure pressure at a single point along the catheter body, which catheter is moveable to detect pressure differential measurements. The invention can be used to more accurately have knowledge of the position of a blood vessel, by means of a heat transfer device.

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1 IMPROVEMENTS RELATING TO CATHETER POSITIONING

2

3 The present invention relates to improvements for the  
4 positioning of catheters monitoring cardiac output  
5 data.

6

7 US 5509424 describes a catheter having a heat transfer  
8 device near its distal end for use in monitoring  
9 cardiac output within an artery. The apparatus  
10 determines cardiac output using selected features  
11 derived from a temperature difference signal based on  
12 measurement of average native blood temperature  
13 detected at a proximal temperature sensor from the  
14 temperature of a heating coil detected by a distal  
15 temperature sensor.

16

17 An important consideration in the use of such catheters  
18 is the importance of the location of the catheter and  
19 its heat transfer device. The main pulmonary artery of  
20 a human is generally only about five centimetres long,

1 and it is important to have the catheter positioned  
2 correctly in order to obtain the correct cardiac output  
3 (CO) information.

4  
5 According to a non published study in 60 patients, the  
6 tip of a catheter, after normal flotation of the  
7 catheter into the main pulmonary artery (PA), could be  
8 between 0-8 cm in the left or right main branch of the  
9 PA. In the case of a catheter that relies on thermal  
10 dilution for the determination of cardiac output (CO),  
11 this positioning is acceptable. However, in the case  
12 of a catheter as described in US 5509424 which relies  
13 on the heat transfer principle for measurement of  
14 cardiac output, the position of the heat transfer  
15 element (HTD) is critical. If the HTD is located in a  
16 branch, then it will sense part of the flow giving a  
17 lower CO. Also if the HTD is near high turbulence, for  
18 example, near a valve or bifurcation, it would give  
19 higher CO. Hence it is important to control the  
20 position of HTD in order to improve the overall  
21 accuracy of CO determination.

22  
23 One design of a cathater according to US 5509424 has a  
24 heat transfer device located at 7.5 cm from the distal  
25 tip (figure 1). This will ensure, based on the  
26 clinical study mentioned above, that the HTD would not  
27 be in a branch in 95% of the cases. However, based on  
28 one clinical study in 20 patients, there appeared to be  
29 a position influence in about 20-30% of the time (CO  
30 determined by heat transfer was significantly lower  
31 than CO determined by thermal dilution).

32

1 It is an object of the present invention to provide  
2 apparatus and method for a catheter for positional  
3 information.

4  
5 According to one aspect of the present invention, there  
6 is provided a catheter which includes means to measure  
7 local pressure at two or more points along the catheter  
8 body.

9  
10 The points are preferably located in two different  
11 pressure areas. The catheter preferably has a heat  
12 transfer device thereon, more preferably at or near its  
13 distal end.

14  
15 The pressure measuring means may be fluid filled lumens  
16 which allow transmission of a pressure waveform to a  
17 pressure transducer which may be located outside the  
18 patient. Alternatively, pressure transduction means  
19 may be located at these points and the signal  
20 transmitted via electrical cables, fluid or fibre  
21 optic. The transduction means itself may be optical,  
22 semiconductor or some other means. The pressure  
23 measuring means may be identical or different. The  
24 transmission could pass along only one lumen.

25  
26 The measuring means is preferably two or more pressure  
27 measuring devices such as diaphragms located along the  
28 length of the catheter body. The information from the  
29 different pressure measuring means can be referenced  
30 and calculated to indicate the position of the  
31 catheter, more particularly the catheter tip and any  
32 heat transfer device, in a blood vessel, organ or  
33 similar. The catheter could use an existing lumen or

1 includes an additional lumen to relay the information  
2 from the pressure measuring means to its proximal end.

3

4 According to a second aspect of the present invention,  
5 there is provided a method of gauging the positional  
6 location of a catheter in a blood vessel, organ or  
7 similar, the catheter having means to monitor the local  
8 pressure at two or more points along the catheter body,  
9 wherein the catheter is located along two different  
10 pressure areas, and the pressure differential  
11 measurements between the points in the two different  
12 areas is indicative of the location of the catheter.

13

14 The pressure detecting means of the present invention  
15 could be located across a valve in a blood vessel,  
16 organ or similar, eg the heart. In one embodiment of  
17 the present invention, one pressure detecting means is  
18 located in the pulmonary artery, and one pressure  
19 detecting means is located in an adjoining ventricle.  
20 The known different pressures of the blood in the  
21 pulmonary artery and the ventricle will create a  
22 pressure differential, and with knowledge of the artery  
23 pressure at the valve, the pressure differential  
24 information can be used to ensure that the catheter tip  
25 and heat transfer device is located where desired, eg  
26 whether the tip is in the atrium, the ventricle or in  
27 the pulmonary artery.

28

29 Typically a catheter according to the present invention  
30 will have means to locate pressure points so that the  
31 heat transfer device is in the centre of the main  
32 pulmonary artery.

33

1 According to a third aspect of the present invention,  
2 there is provided a method of gauging the positional  
3 location of a catheter in a blood vessel, organ or  
4 similar, the catheter having means to monitor the local  
5 pressure at a point along the catheter body, wherein  
6 the catheter is located in a first position in the  
7 vessel, organ or similar, and the local pressure  
8 measured, and the catheter is then moved to a second  
9 position in the vessel, organ or similar, and the local  
10 pressure measured, and the pressure measurements at the  
11 first and second locations are indicative of the  
12 location of the catheter.

13

14 This method would use only one pressure measuring means  
15 to detect the pressure waveforms. This allows  
16 minimising the size of a catheter for applications  
17 requiring the least possible outer diameter, for  
18 example in paediatric or neonatal cardiovascular  
19 system. The catheter would be moved forward until the  
20 indicative pressure waveform (measured by the pressure  
21 measuring means) changed indicating that the sensor had  
22 crossed a valve. The catheter could then be withdrawn  
23 until the valve is crossed again, to confirm the  
24 position. In this way any part of the catheter at  
25 fixed, known distances from the pressure sensing means  
26 can have location known relative to the position of the  
27 valve.

28

29 In a preferred embodiment, the catheter could have  
30 calibrated distance markings on its outer surface to  
31 assist in accurate determination of insertion and  
32 withdrawal distances.

33



1 According to a fourth aspect of the present invention  
2 there is provided a catheter which includes internal  
3 fluid piping whose fluid pressure is relatable to the  
4 general pressure of surrounding fluid external to the  
5 catheter, and at least one means to measure the fluid  
6 pressure in the internal piping.

7  
8 The piping could directly use a portion of the fluid  
9 surrounding the catheter. Alternatively, the piping  
10 could relay information from an external pressure  
11 measuring means such as a diaphragm. The catheter  
12 preferably has a heat transfer device at or near its  
13 distal end.

14  
15 Embodiments of the present invention are shown by way  
16 of example only in the accompanying diagrammatic  
17 drawings in which;

18  
19 Figure 1 is a cross-sectional view through part of a  
20 first catheter according to the present invention;

21  
22 Figure 2 is a cross-sectional view through a part of a  
23 second catheter according to the present invention; and

24  
25 Figure 3 shows R.V. and PA traces provided by the  
26 catheter shown in Figure 2.

27  
28 Figure 4 illustrates positioning of a Pulmonary Artery  
29 Catheter.

30  
31 Referring to the drawings, Figure 1 is a cross  
32 sectional view of a section of a first catheter 2,  
33 having an internal fluid piping 4. Each end of the

7

1 piping 4 is covered by a diaphragm 6 aligned with the  
2 catheter outer wall 8. The piping 4 is filled with a  
3 fluid 10 such as a sterile saline solution or gel. The  
4 fluid should be non-toxic and bio-compatible.

5

6 In the middle of the piping 4 is a third diaphragm 11  
7 connected to a pressure sensor (not shown) at the end  
8 of a lumen 14.

9

10 In use, this section of the catheter 2 is intended to  
11 be located across a differential pressure boundary  
12 (dashed line A-A) such as a heart ventricle valve, such  
13 that the pressure on one of the end diaphragms 6 of the  
14 piping 4 is different to that on the other. The  
15 different pressures on the end diaphragms 6 will result  
16 (through the internal fluid 10) in movement of the  
17 intermediate diaphragm 11, and movement of this  
18 diaphragm 11 can be measured by the pressure sensor.

19

20 With knowledge of the blood pressure at and around the  
21 heart, positive confirmation of the correct location of  
22 the catheter 2 can be provided by waiting for the  
23 desired pressure measurement to be sensed, confirming  
24 the location of the piping 4 across a valve. The  
25 precise position of the catheter tip and any associated  
26 heat transfer device can then be confirmed, also  
27 allowing correct determination of information relating  
28 to the heat transfer device.

29

30 Figure 2 shows a second catheter body 12 which has two  
31 measuring means 13, 14, with respective waveform  
32 transmissions means 13a, 14a. The dashed line BB  
33 indicates a pulmonary valve. The pressure waveform

8

1 trace measured at position 13 would be as shown in  
2 Figure 3; the waveform indicative of the right  
3 ventricle, R.V. Similarly, position 14 would show the  
4 waveform indicative of the pulmonary artery PA also  
5 shown in Figure 3. When the catheter 12 was so  
6 positioned as to give these respective waveforms the  
7 user would know the location of the pressure measuring  
8 means 13, 14 and hence the location of any other part  
9 of the catheter 12 which is a fixed distance along the  
10 catheter from those means. For example, if the distal  
11 tip 16 was 10 cm from point 14, then the user would  
12 know that the tip was approximately 10 cm from the  
13 pulmonary valve. Similarly for a heat transfer device  
14 15, located for example 1cm from point 14.

15

16 Figure 4 illustrates positioning of a pulmonary artery  
17 catheter. The catheter (2) extends through the  
18 Superior Vena Cava (17), into the Right Atrium (18),  
19 into the Right Ventricle (19), into the Main Pulmonary  
20 Artery (20) and into the Right Pulmonary Branch (21).  
21 Use of pressure detecting means allows the heat  
22 transfer device to be positioned in the main pulmonary  
23 artery.

24

25 The present invention provides two approaches for  
26 actual clinical practice;

27

28 Approach 1

29

30 Provide a separate lumen for pressure monitoring. A  
31 current catheter according to US Patent No 5509424 has  
32 a cross section having 6 lumens described as follows:

33

1 The proximal injectate lumen terminates at a port  
2 located 30 cm from the distal tip. When the  
3 distal tip is located in the pulmonary artery, the  
4 proximal injectate port resides in the right  
5 atrium or vena cava, allowing for bolus cardiac  
6 output injections, right arterial pressure  
7 monitoring, blood sampling, or infusion of  
8 solutions.

9  
10 The pulmonary artery (PA) distal infusion lumen  
11 terminates at the distal tip. During insertion,  
12 this port is used to monitor catheter location,  
13 via transitional pressure measurements. At full  
14 insertion, this port resides in the pulmonary  
15 artery, (allowing for pulmonary artery and  
16 pulmonary capillary wedge pressure measurements)  
17 or mixed venous blood sampling. This port also  
18 allows for infusion of solutions, pressure  
19 monitoring or blood sampling.

20  
21 The distal and proximal thermistor lumens contain  
22 the electrical leads for the thermistors, which  
23 are positioned on the catheter surface,  
24 approximately 7.5 cm and 11 cm respectively from  
25 the distal tip. The thermistors are used to  
26 measure temperatures and in conjunction with the  
27 thermal coil, generate data used to calculate  
28 cardiac output. The distal thermistor is located  
29 immediately below the thermal coil.

30  
31 The thermal coil lumen contains leads for the  
32 thermal coil, which is located 7.5 cm from the  
33 distal tip. The thermal coil generates heat

10

1 necessary for maintenance of a constant  
2 temperature differential between the proximal and  
3 distal thermistors. The energy required to  
4 maintain the fixed temperature differential, is  
5 used to calculate cardiac output continuously.

6  
7 The balloon inflation lumen has a one-way stopcock  
8 at its proximal end and terminates in a latex  
9 balloon at the distal tip. When the catheter is  
10 properly positioned in the pulmonary artery, the  
11 balloon is inflated intermittently for the  
12 measurement of pulmonary artery wedge pressure.  
13 The balloon is inflated by a volume restricted  
14 syringe.

15

16 By combining the two thermistors and coil wires in one  
17 lumen, two lumens become available to be used for  
18 pressure monitoring.

19

20 In the first approach there is a slot (PC1) at 3cm  
21 below the heat transfer device (HTD), in one of the two  
22 vacated lumens, and another slot (PC2), in the second  
23 vacated lumen, at 2 cm above HTD. When the catheter is  
24 floated in place, the trace of PC1 should be PA  
25 waveform, and PC2 should be the right ventricular (RV)  
26 waveform if the HTD is located in mid PA. Manipulation  
27 of catheter position to achieve these traces ensures  
28 always locating the HTD in the right place.

29

30 Approach 2

31

32 Another approach would be to vacate only one lumen to  
33 use only one slot either below or above the HTD.

1

2 A. For example, if the pressure slot is located 3-4  
3 cm below the HTD, the catheter can be advanced  
4 until this pressure slot shows a PA trace, then it  
5 is withdrawn slightly (e.g. 1 cm increments) until  
6 an RV trace is obtained. The HTD will then be in  
7 the main PA just after the pulmonic valve.

8

9 B. Or, the slot is placed 2 cm above the HTD. When  
10 the catheter is in place, withdraw catheter until  
11 an RV trace is observed, then advance 4 cm into  
12 PA. The HTD is then in the main PA above the  
13 pulmonic valve.

14

15

16 The present invention can be used to more accurately  
17 have knowledge of the position of the catheter in a  
18 blood vessel, organ or similar. Where the catheter  
19 includes a heat transfer device, the position of the  
20 heat transfer device can be more accurately calculated,  
21 and thus the nature of the heat measurements and  
22 associated cardiac information can be more accurately  
23 determined.

24

25 Particular applications for this invention include:

26

27 ensuring that a component is located in the  
28 pulmonary artery

29

30 ensuring that a component is located in the right  
31 ventricle

32

12

1 ensuring that the distal tip of a product is not  
2 more than a certain distance beyond the pulmonary  
3 valve.  
4

5 The last point is relevant to any pulmonary artery  
6 catheter. It is important for the wellbeing of  
7 patients that the tip of any pulmonary artery catheter  
8 is not allowed too far beyond the pulmonary valve.  
9

10 The novel apparatus and methods of the present  
11 invention could also be used in non-medical fields  
12 requiring accurate positioning of elongate tubing and  
13 the like in remote locations. Such fields include  
14 aeronautics, any fluid flow analysis, food and drink  
15 processing and monitoring, water and sewerage  
16 management, chemical engineering, fuel supply to  
17 engines, etc. Indeed, the present invention is also  
18 applicable to any device required to be placed beyond a  
19 one-way valve in a fluid flow situation, and/or any  
20 fluid flow situation which exhibits a pressure  
21 differential.

1   Claims

2

3    1.    A catheter having a catheter body, wherein the  
4           body includes means to measure local pressure at  
5           two or more points along the catheter body.

6

7    2.    A catheter as claimed in Claim 1 wherein the  
8           measuring means comprises two or more pressure  
9           measuring devices located along the length of the  
10          catheter body.

11

12   3.    A catheter as claimed in Claim 2 wherein the  
13          pressure measuring devices are diaphragms.

14

15   4.    A catheter as claimed in Claim 1 wherein the means  
16          comprises one or more fluid-filled lumens or  
17          piping.

18

19   5.    A catheter as claimed in Claim 4 having one or  
20          more intermediate diaphragms across the or each  
21          lumen or piping.

22

23   6.    A catheter as claimed in any one of the preceding  
24          Claims which includes a pressure transduction  
25          means.

26

27   7.    A catheter as claimed in Claim 6 which includes  
28          signal transmission means able to transmit local  
29          pressure information from one or more points along  
30          the catheter body to the proximal end of the  
31          catheter.

32



- 1 8. A catheter as claimed in 7 wherein the signal is  
2 transmitted via one or more electrical cables,  
3 fluid or fibre optic.  
4
- 5 9. A catheter as claimed in any one of the preceding  
6 Claims wherein pressure measurement information is  
7 passed along the catheter through one or more  
8 lumens in the catheter body.  
9
- 10 10. A catheter as claimed in any one of the preceding  
11 Claims which includes one or more heat transfer  
12 devices.  
13
- 14 11. A method of gauging the positional location of a  
15 catheter in a blood vessel, organ or similar, the  
16 catheter having means to monitor the local  
17 pressure at two or more points along the catheter  
18 body, wherein the catheter is located along two  
19 different pressure areas, and the pressure  
20 differential between the points in the two  
21 different areas is indicative of the location of  
22 the catheter.  
23
- 24 12. A method as claimed in Claim 11 wherein the  
25 pressure monitoring means is located across a  
26 valve in a blood vessel organ or similar.  
27
- 28 13. A method as claimed in Claim 12 wherein the  
29 pressure monitoring means is located across a  
30 valve in the heart.  
31
- 32 14. A method of gauging the positional location of a  
33 catheter in a blood vessel, organ or similar, the

15

1 catheter having means to monitor the local  
2 pressure at a point along the catheter body,  
3 wherein the catheter is located in a first  
4 position in the vessel, organ or similar, and the  
5 local pressure measured, and the catheter is then  
6 moved to a second position in the vessel organ or  
7 similar, and the local pressure measured, and the  
8 pressure measurements at the first and second  
9 locations are indicative of the location of the  
10 catheter.

11

12 15. A method as claimed in Claim 14 for a paediatric  
13 or neo-natal catheter.

14

15 16. A method as claimed in Claim 14 or Claim 15  
16 wherein the catheter is located in a first  
17 position on one side of a valve, and in the second  
18 position on the other side of the valve.

19

20 17. A method as claimed in any one of Claims 14-16  
21 wherein the catheter has calibrated distance  
22 markings on its outer surface.

23

24 18. A catheter which includes internal fluid piping  
25 whose fluid pressure is relatable to the general  
26 pressure of surrounding fluid external to the  
27 catheter, and at least one means to measure the  
28 fluid pressure in the internal piping.

29

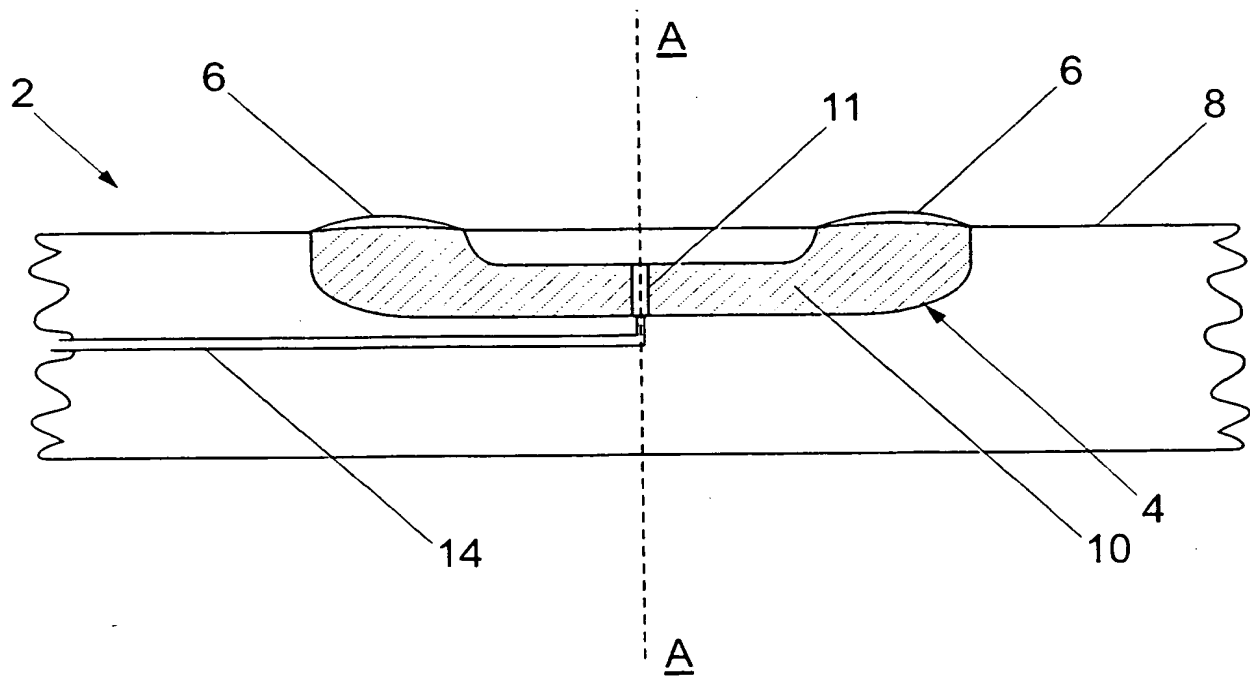
30 19. A catheter as claimed in Claim 18 wherein the  
31 piping uses a portion of the fluid surrounding the  
32 catheter.

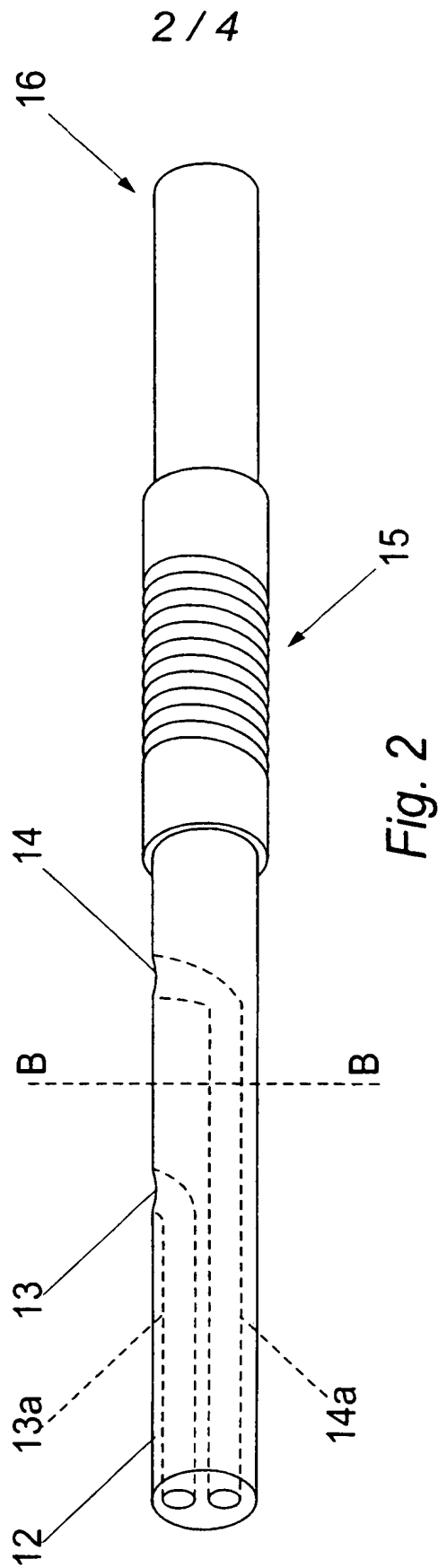
33

16

- 1 20. A catheter as claimed in Claim 18 wherein the  
2 piping relays information from an external  
3 pressure measuring means.  
4
- 5 21. A catheter as claimed in Claim 20 wherein the  
6 external pressure measuring means is a diaphragm.  
7
- 8 22. A catheter as claimed in any one of Claims 18-21  
9 which includes a heat transfer device at or near  
10 its distal end.  
11
- 12 23. A catheter as claimed in any one of Claims 1 to 10  
13 and 18-22 for use in any one of: aeronautics,  
14 fluid flow analysis, food and drink processing and  
15 monitoring, water and sewage management, chemical  
16 engineering, fuel engine supply.  
17

1 / 4

*Fig. 1*



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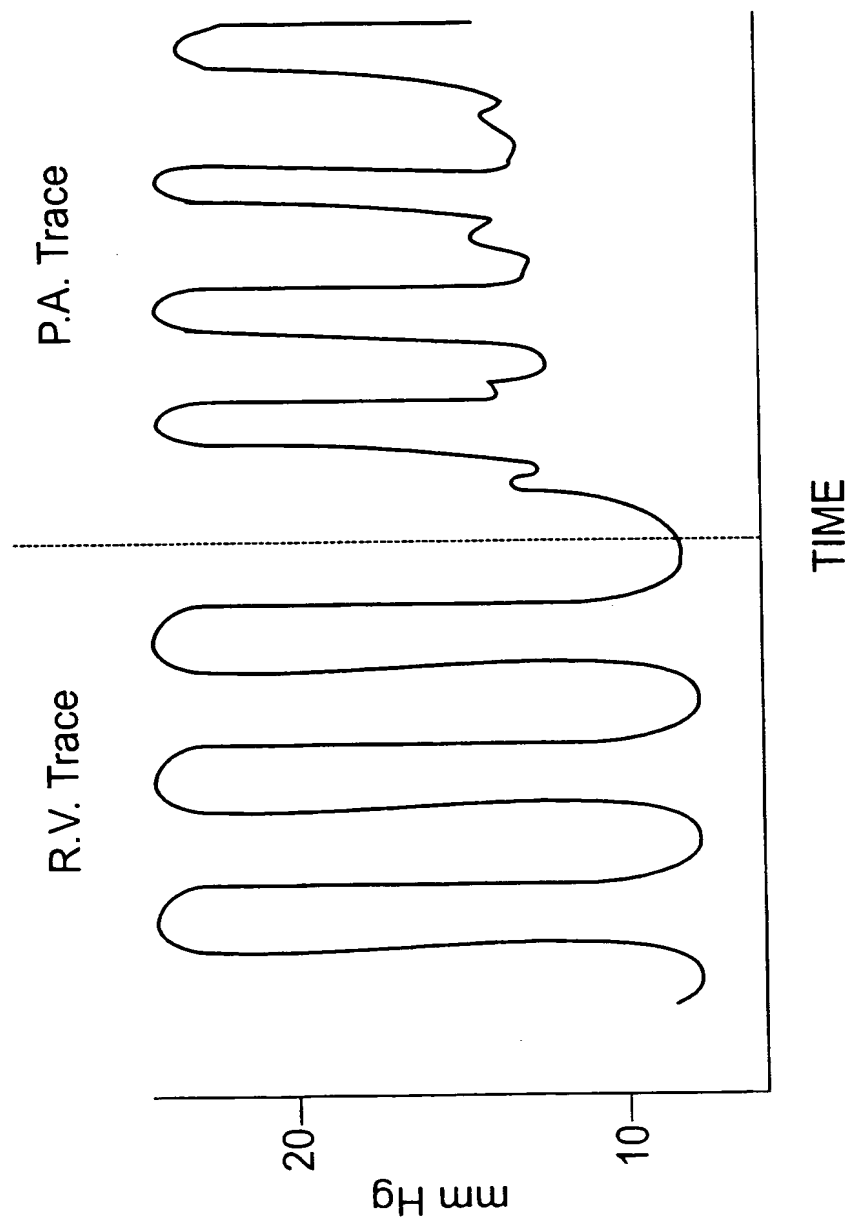
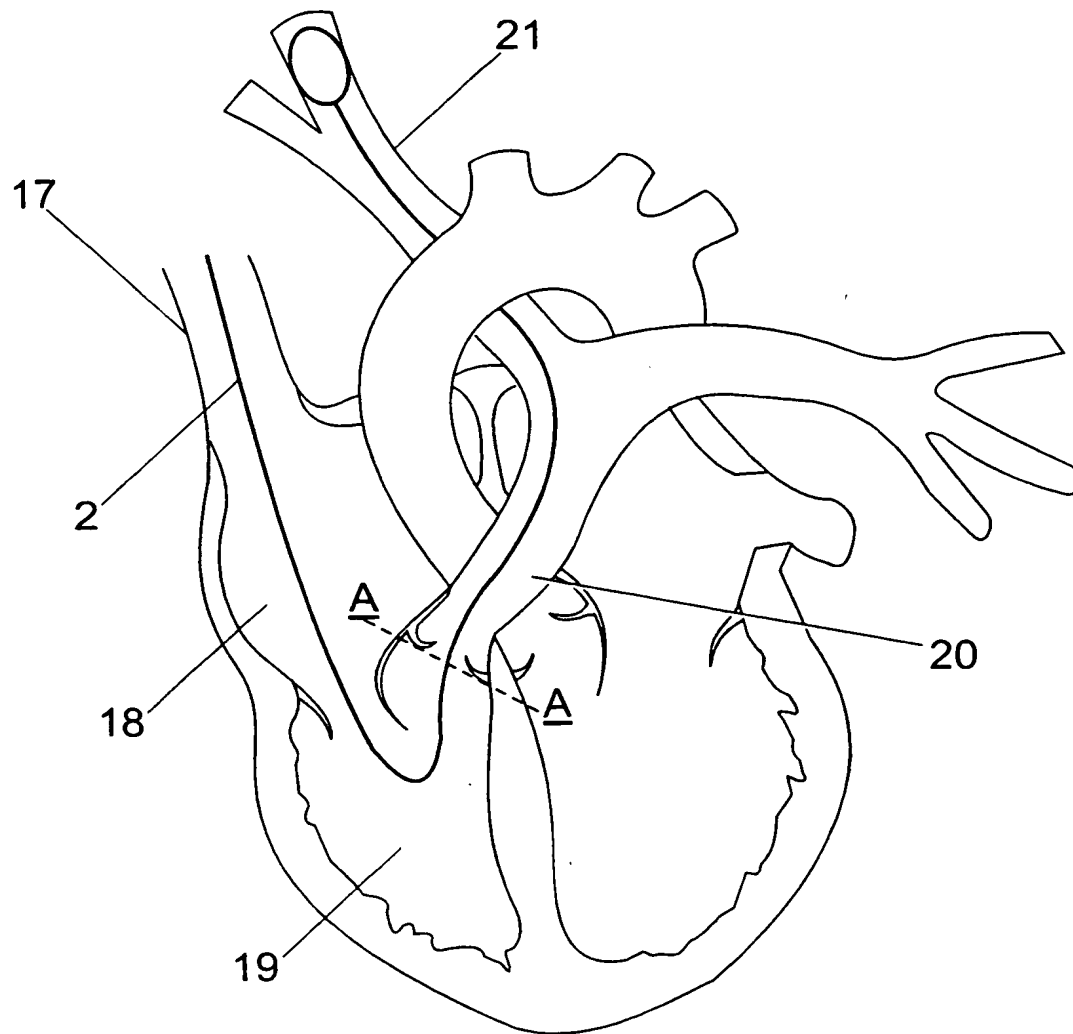


Fig. 3

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*Fig. 4*

# INTERNATIONAL SEARCH REPORT

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A. CLASSIFICATION OF SUBJECT MATTER  
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According to International Patent Classification (IPC) or to both national classification and IPC

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## C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X A	EP 0 363 117 A (BAXTER INT) 11 April 1990 (1990-04-11)  column 5, line 26 -column 8, line 45; tables 1-5 ---	1,2,4-9, 11-14, 16-18 3,10,19, 22
X A	US 5 025 786 A (SIEGEL SHARON B) 25 June 1991 (1991-06-25) column 3, line 7 -column 4, line 24; table 1 ---	1,2,8  11-14
X A	US 4 815 472 A (WISE KENSALL D ET AL) 28 March 1989 (1989-03-28) abstract column 13, line 51 -column 14, line 68; table 11 --- -/--	1,2,8  11-14

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☒ Patent family members are listed in annex.

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# INTERNATIONAL SEARCH REPORT

International Application No  
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